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- 1 Short Communication (word count abstract + manuscript: 1199)
- 2 **Title:**
- 3 Executive function orchestrates regulation of task-relevant gait fluctuations
- 4
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19 Abstract:

- 20 Humans apply a minimum intervention principle to regulate treadmill walking, rapidly
- 21 correcting fluctuations in the task-relevant variable (step speed: SS) while ignoring
- 22 fluctuations in the task-irrelevant variables (step time: ST; step length: SL). We examined
- 23 whether the regulation of fluctuations in SS and not in ST and SL relies depends on high-
- 24 level, executive function, processes. Young adults walked on a treadmill without a cognitive
- 25 requirement and while performing the cognitive task of dichotic listening. SS fluctuations
- 26 became less anti-persistent when performing dichotic listening, meaning that taxing
- 27 executive function impaired the ability to rapidly correct speed deviations on subsequent
- steps. Conversely, performing dichotic listening had no effect on SL and ST persistent
- 29 fluctuations. Findings suggest that high-level brain processes are only involved only in
- 30 regulating gait task-relevant variables.
- 31

32 Key-Words:

33 Walking; Variability; Minimum Intervention Principle; Executive Function; Detrended

34 Fluctuation Analysis

35 **1. Introduction**

In a wide range of tasks, humans apply a minimum intervention principle to regulate
 movement, correcting fluctuations only if they interfere with task performance [1,2]. This
 control holds because correcting task-irrelevant fluctuations in addition to task-relevant
 fluctuations has detrimental effects on the central nervous system (CNS), increasing noise
 and computational effort.

- 41 In gait, such a principle has been demonstrated by examining the statistical 42 persistence/anti-persistence of the stride-to-stride fluctuations during treadmill walking [3,4]. 43 Specifically, fluctuations in stride time and stride length were found to be persistent, meaning 44 that their values continued increasing or decreasing over several subsequent strides before 45 reversing. Colnversely, fluctuations in stride speed were anti-persistent, rapidly 46 reversing direction on subsequent strides. Given that the treadmill walking task requires 47 maintaining (on average) the same walking speed (to not walkavoid walking off the treadmill) 48 and that many combinations of stride length and stride time equally achieve that speed, only
- 49 task-relevant fluctuations only were therefore were immediately corrected.
- 50 However, the question remains as to whether persistent and anti-persistent
- 51 fluctuations stem from similar or different control processes of the CNS. Interestingly, only
- 52 <u>anti-persistence in step speed is needed to achieve the treadmill walking goal (to maintain</u>
- 53 constant walking speed [3,4]). Accordingly, high-level executive function processes, which
- 54 are involved in handling goal-directed actions [5], may only play a role only in shaping anti-
- 55 persistent behavior. If trueso, taxing these processes by with a concurrent cognitive task
- 56 during treadmill walking would alter anti-persistence in step speed while persistence in step
- 57 time and step length would remain unchanged.

58 **2. Methods**

59 Twenty healthy adults (12²/8³, 24.45±0.87 years, 1.73±0.02 m, 70.41±2.63 kg) 60 participated in two experimental sessions after providing written informed consent. The 61 experiment included The order of the two sessions was -counterbalanced between subjects. 62 In one session, subjects performed the cognitive task of dichotic listening while being seated 63 to establish baseline performance [6,7]. They had to listen and report consonant-vowel 64 syllables (phonologically salient, but semantically meaningless) presented dichotically under 65 three attention conditions: non-forced (NF) consisted in reporting the syllable heard best, and 66 forced-right (FR) and forced-left (FL) the syllable heard in the right and left ear, respectively. The conditions increased in the need of for executive control, from NF to FL. In the other 67 68 session, subjects walked on a treadmill at preferred speed (1.06±0.03 m/s) with markers 69 attached at anatomical landmarks [8], first without a cognitive requirement (walking: W) and 70 afterwards while performing dichotic listening in NF (W+NF), FR (W+FR) and FL (W+FL) (Fig.

- 1). In both sessions, NF was presented first and FR and FL were counterbalanced between
 subjects. Each condition lasted for three minutes, involving 36 different syllable pairs. Eprime® was used for syllable presentation and report collection. The marker movements
 were recorded (60 Hz) with an 8-camera Motion Analysis Eagle Digital system and low-pass
 filtered at 10 Hz with a zero-lag Butterworth filter.
- 76

----- Please insert Figure 1 here -----

77 Dichotic listening was scored through the laterality index (LI), which is the ratio of the 78 difference between correct reports for the right ear and those for the left ear to the total 79 number of correct reports, expressed in as a percentage. Step time (ST) and step length (SL) 80 were defined as the time interval and horizontal distance between consecutive toe-off events. 81 with the toe-off defined from the maximum backward displacement of the marker located 82 between the second and third metatarsal phalangeal joints during each step. Step speed 83 (SS) was defined as SS=SL/ST. The time series were shortened to 272 data points (the 84 number of steps of the slowest subject). Persistence/anti-persistence in ST, SL and SS was 85 examined using Detrended Fluctuation Analysis (DFA) [9,10]. DFA computes computed mean square roots of detrended residuals, F(n), of the integrated time series over a range of 86 87 interval lengths, n. The scaling exponent α is was then estimated from the slope of the linear 88 relationship between log[F(n)] and log(n). A restricted range of interval lengths was used, 89 from n=17 steps to n=45 steps, where the slope was the most stable as determined by the 90 DFBETA statistics [10] (Fig. 2). α <0.5 indicates anti-persistence, with fluctuations in one 91 direction immediately followed by corrections in the opposite direction. α >0.5 indicates 92 persistence, with fluctuations in one direction followed by fluctuations in the same direction. 93 LI and α were subjected to two-way (session \times condition) and one-way (condition) within-

94 subjects analyses of variance (ANOVAs), respectively.

95 ------ Please insert Figure 2 here -----

96 **3. Results**

97 <u>Cognition.</u> There was a *condition* effect for LI ($F_{2,38}=32.91$, $p<10^{-9}$, $\eta^2=0.44$), which 98 increased from NF (11.27±3.29%) to FR (43.65±3.13%; p=0.003) and decreased from FR to 99 FL (-9.08±4.93 %; p<0.001) (Fig. 3A). As previously found, subjects reported more correct 100 answers at-for the right ear in NF and FR, and inversely reported more correct answers at-for 101 the left ear in FL [7]. The ANOVA did not reveal a *session* effect for LI, meaning that 102 cognitive performance was maintained during walking.

- 103 <u>*Gait.*</u> DFA revealed anti-persistence in SS (α <0.5) and persistence in ST and SL 104 (α >0.5). The ANOVA yielded a *condition* effect for α (SS) ($F_{2.44}$ =4.71, p=0.01, η ²=0.12).
- 105 Fluctuations were less anti-persistent in W+FL (α =0.45±0.04) than in W (α =0.31±0.03,

106 p=0.006) and W+NF (α =0.34±0.03, p=0.041). There were no significant results for α (ST) and 107 α (SL) (Fig. 3B).

108 ------ Please insert Figure 3 here -----

109 **4. Discussion**

110 This study examined the origins of persistent/anti-persistent fluctuations in gait. As 111 expected, taxing the executive function processes with dichotic listening led to less anti-112 persistent SS, which reflected an impaired ability to rapidly correct speed deviations on 113 subsequent steps. Therefore, executive function was involved in regulating anti-persistence 114 in the variable relevant for achieving the treadmill walking goal (to maintain constant speed 115 [3,4]). Interestingly, a previous model of gait dynamics reproduced anti-persistent fluctuations 116 in ST (the task-relevant variable) during metronomically-paced walking [11,12]. The authors 117 suggested that anti-persistence resulted from the "human consciousness" of being 118 constrained to walk at a controlled pace by following external timing cues. Accordingly, our 119 finding supports the proposal that anti-persistence in gait results from high-level brain 120 processes. 121 Conversely, decreasing the cognitive resources available had no effect on the 122 persistence of the task-irrelevant variables for treadmill walking (ST and SL). Accordingly, the 123 persistent fluctuations likely stem likely from low-level processes of the CNS and the inherent 124 biomechanics of the locomotor system. This interpretation is in agreement with modelling 125 studies that reproduced persistent fluctuations in ST using either an intra-spinal network of 126 neurons coupled, or not, to a mechanical oscillator [9,11-14] or a biomechanical model of 127 walking operating under minimal feedback (spinal reflex) [15]. 128 In sum, high-level brain processes were only involved in regulating anti-persistent 129 speed fluctuations. This finding suggests that the minimum intervention principle minimizes 130 the cognitive cost of locomotion by tightly regulating solely only step speed, the variable that 131 is directly relevant to achieving the task goal. 132

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- 174 Legends
- 175 176

177 Fig. 1. Experimental setup with a subject walking on the treadmill while performing the 178 dichotic listening test. Consonant-vowel syllables /ba/, /da/, /ga/, /pa/, /ta/, and /ka/ were 179 presented as stimulus-pairs (e.g., /ga/-/ba/) using a headphone, one syllable to the right ear 180 (e.g., /ga/) and simultaneously the other syllable to the left ear (e.g., /ba/). The subjects were 181 asked to freely report the consonant-vowel syllable they heard best from the dichotic syllable 182 pair in the non-forced (NF) condition (e.g., /ga/, assuming a right ear advantage). On the 183 other hand, they were instructed to report only the syllable presented to the right ear in the 184 forced-right (FR) condition (e.g., /ga/) and to the left ear in the forced-left (FL) condition (e.g., 185 /ba/). The subjects were secured into the LiteGait® harness system for a safety purposes. 186 Reflective markers were attached to specific anatomical landmarks, including the anterior 187 and posterior superior iliac spine, lumbosacral joint, greater trochanter of the femur, lateral 188 mid-thigh, front lower thigh, lateral and medial epicondyles of the femur, front mid-shank, 189 lateral lower shank, lateral and medial malleoli, lateral border of the fifth metatarsal head, 190 medial border of the first metatarsal head, lateral and medial processes of the calcaneal 191 tuberosity, heel, and between the second and third metatarsal phalangeal joints.

192 193

194 Fig. 2. (A) Step length (SL), step time (ST) and step speed (SS) time series (N=272 steps) 195 obtained from a representative subject walking at preferred speed. (B) Corresponding log-log 196 plots of average fluctuations F(n) vs. interval lengths n, obtained using the Detrended 197 Fluctuation Analysis. The $log_{10}[F(n)]$ vs. $log_{10}(n)$ plots were fitted with linear functions and the 198 scaling exponents α were obtained from the slopes of these lines over the range of interval 199 lengths n=17 to n=45. This range provided the most stable estimates of α for SL, ST, and SS. 200 As illustrated, step-to-step fluctuations of both SL and ST time series were persistent (α >0.5) 201 while those of SS time series were anti-persistent (α <0.5). (C) The stable interval length 202 fitting range was determined from the distribution of the diagnostic measure DFBETA, which 203 reflects how much the exponent α changes when sequentially removing the intervals of 204 length n. The values presented here are means ± standard deviations of the population. For 205 small interval lengths (n<17data points), the DFBETA values exhibited bias away from zero 206 and were importantly dispersed, reflecting estimations of α over- or under-estimated and 207 poorly stable, respectively. Indeed, small intervals contain few data points for fitting the 208 trends, which likely render the α estimates inaccurate and variable. For large interval lengths 209 (n>45 data points), the DFBETA values did not exhibit bias but were importantly highly 210 dispersed. These interval lengths provide sufficient data for fitting to fit the trend but the

6

- 211 average fluctuations around the trends are more variable, making the α estimates less stable.
- 212 Therefore, the restricted range of lengths $17 \le n \le 45$ was considered for estimating α .
- 213
- 214 Fig. 3. (A) Laterality indexes (LI) obtained in the dichotic listening conditions (NF: non-forced,
- 215 FR: forced-right, FL: forced-left) during the sitting and walking sessions. Results from the
- 216 two-way within-subjects ANOVAs (*Condition*×Session) indicated a significant main effect of
- 217 condition for LI, with the p-value for the effect p_c reported on the graph. (B) Exponents α
- obtained from step length (SL), step time (ST), and step speed (SS) time series as a function
- 219 of the experimental conditions (walking: W, walking when performing dichotic listening:
- 220 W+NF, W+FR, and W+FL). Results from the one-way within-subjects ANOVAs indicated a
- significant main effect of *condition* for $\alpha(SS)$, with the p-value for the effect $p_c(SS)$ reported
- 222 on the graph. LI and α values are means \pm standard errors of the population.