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# Frontal joint dynamics when initiating stair ascent from a walk versus a stand

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1           **Frontal Joint Dynamics when Initiating Stair Ascent from a Walk versus a Stand**  
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23 **Abstract**

24 Ascending stairs is a challenging activity of daily living for many populations. Frontal plane  
25 joint dynamics are critical to understand the mechanisms involved in stair ascension as they  
26 contribute to both propulsion and medio-lateral stability. However, previous research is limited  
27 to understanding these dynamics while initiating stair ascent from a stand. We investigated if  
28 initiating stair ascent from a walk with a comfortable self-selected speed can affect the frontal  
29 plane lower-extremity joint moments and powers as compared to initiating stair ascent from a  
30 stand and if this difference would exist at consecutive ipsilateral steps on the stairs. Kinematics  
31 data using a 3-D motion capture system and kinetics data using two force platforms on the first  
32 and third stair treads were recorded simultaneously as ten healthy young adults ascended a  
33 custom-built staircase. Data were collected from two starting conditions of stair ascent, from a  
34 walk (speed:  $1.42 \pm 0.21$  m/s) and from a stand. Results showed that subjects generated greater  
35 peak knee abductor moment and greater peak hip abductor moment when initiating stair ascent  
36 from a walk. Greater peak joint moments and powers at all joints were also seen while ascending  
37 the second ipsilateral step. Particularly, greater hip abductor moment was needed to avoid  
38 contact of the contralateral limb with the intermediate step by counteracting the pelvic drop on  
39 the contralateral side. This could be important for therapists using stair climbing as a  
40 testing/training tool to evaluate hip strength in individuals with documented frontal plane  
41 abnormalities (i.e. knee and hip osteoarthritis, ACL injury).

42 **Keywords: Stair climbing; Joint moments; Joint powers; Walking; Stair ambulation;**  
43 **Abductor Muscles; Adductor Muscles**

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## 46 **1. Introduction**

47 Older adults frequently experience falls while negotiating stairs (Rubenstein 2006;  
48 Hemenway et al., 1994). Hence, understanding fall-related mechanisms via examining the joint  
49 dynamics (moments and powers) has been a research area of great interest (McFadyen and  
50 Winter, 1988; Startzell et al., 2000; Reeves et al., 2008). Particularly, the frontal plane dynamics  
51 contribute to both propulsion and medio-lateral stability (Nadeau et al., 2003; Novak and  
52 Brouwer, 2011) and are critical at the knee and hip joints (Andriacchi et al., 1980; Kowalk et al.,  
53 1996; Costigan et al., 2002). These two joints experience external adductor moments (Kowalk et  
54 al., 1996) and compared to level-walking, these moments are lesser at the hip and greater at the  
55 knee (Costigan et al., 2002; Nadeau et al., 2003). These moments have also been shown to be  
56 similar for two consecutive steps (Kowalk et al., 1996). Examining the frontal plane dynamics  
57 during stair negotiation could play a pivotal role in rehabilitation of people with weak hip  
58 abductors and with knee problems (Nadeau et al., 2003).

59 Importantly, the currently available literature only includes studies where stair ascent was  
60 initiated from a stand. However, initiating stair ascent from a walk is much more common at  
61 private and public locations. Thus to increase external validity in the stair negotiation research, it  
62 is important to consider such a condition. Such an approach immediately generates several  
63 crucial questions: Does ascending stairs from a walk require greater moments and more power to  
64 maintain frontal plane stability as compared to initiating stair ascent directly from a stand? And  
65 if such differences exist, are they present only at the first step of the staircase or also at the next  
66 ipsilateral step? Previous work has shown that ascending stairs starting from a walk caused  
67 higher peak knee and hip extensor moments in the sagittal plane as compared to starting stair  
68 ascent from a stand and altered lower-extremity joint moments and powers between two

69 consecutive ipsilateral steps (Vallabhajosula et al., in press). Such differences could also result in  
70 different joint moments and powers to maintain medio-lateral stability during stair ascent after  
71 starting from a walk or a stand. Therefore, the objective of the present study was to determine  
72 frontal plane joint dynamics when one ascends stairs from a walk compared to ascending stairs  
73 from a stand. Due to enhanced momentum when initiating stair ascent from a walk (increased  
74 velocity) compared to initiating stair ascent from a stand, we hypothesized that the frontal plane  
75 joint moments and powers will be greater when 1) ascending stairs from a walk and 2) at the next  
76 ipsilateral step.

## 77 **2. Methods**

78 Ten healthy subjects (three females;  $26.4 \pm 3.7$  years;  $76.2 \pm 13.6$  kg;  $1.78 \pm 0.08$  m) signed an  
79 informed consent approved by the local institutional review board. Inclusion criteria were: age  
80 between 19-35 years and free of any injury that could alter gait. Exclusion criteria were: presence  
81 of any known disorder(s) that may affect gait or the inability to negotiate a stairway.

82 Kinematic (Motion Analysis Corp., Santa Rosa, CA; 60 Hz) and kinetic data using two  
83 force platforms embedded in the first and the third stair treads of an instrumented stairway  
84 (Advanced Mechanical Technology Inc., Watertown, MA; 600 Hz) were collected (Figure 1).  
85 The force platforms were isolated from the rest of the structure to avoid vibration artifacts  
86 (similar to Holsgaard-Larsen et al., 2011).

87 Retro-reflective markers were placed on subjects' pelvis and lower limbs based on  
88 modified Helen Hayes marker set (Houck et al., 2005). Before testing, all the subjects were  
89 allowed to practice stair ascension without using handrails. During testing, none of the subjects  
90 used the handrails. Subjects wore comfortable sport shoes and walked towards the stairs at their  
91 self-selected comfortable speed from a distance of 5m. Their speed was calculated based on the

92 time recordings of two photocells positioned 2m apart in front of the stairway (Figures 2A,2B).  
93 An average walking speed ( $1.42\pm 0.21\text{m/s}$ ) from 16 such trials was used as the self-selected  
94 comfortable speed for each subject. Next, the subjects ascended stairs five times in two  
95 conditions, starting with the right limb for each condition: 1) initiating stair ascent from a walk  
96 (condition 1; Figures 2A,2B), and 2) initiating stair ascent from a stand (condition 2; Figures  
97 2C,2D). An acceptable trial for condition 1 required the subject to ascend the stairway within  
98  $\pm 10\%$  of the self-selected comfortable speed. Data were collected until five acceptable trials  
99 were procured. The order of the conditions was randomized.

100 Peak internal abductor and adductor moments, and peak power generated and absorbed at  
101 ankle, knee, and hip joints were used as the dependent variables (Costigan et al., 2002; Nadeau et  
102 al., 2003). They were calculated for two consecutive ipsilateral steps on the staircase during both  
103 conditions using a custom-written Matlab (MathWorks Inc., Natick, MA, USA) program. For  
104 each subject, and for each condition, the maximum and minimum joint moments and powers  
105 from the five trials were averaged to calculate the mean values. Group means and standard  
106 deviations were then obtained by averaging these mean peak values. A fully repeated two-way  
107 ANOVA (condition X step) was performed using SPSS (International Business Machines,  
108 Armonk, NY) with  $\alpha$ -value set at 0.05.

### 109 **3. Results**

110 Subjects produced significantly greater peak abductor moments at the knee (3%;  $P=0.014$ )  
111 and hip (7%;  $P=0.006$ ) when initiating stair ascent from a walk (Figure 3A). Subjects produced  
112 significantly greater peak ankle (20%;  $P=0.007$ ), knee (20%;  $P<0.001$ ) and hip abductor  
113 moments (20%;  $P<0.001$ ) at the second ipsilateral step (Figure 3B). There were no significant  
114 interactions.

115 Subjects generated significantly greater peak power at the ankle (48%;  $P=0.023$ ), knee (43%;  
116  $P=0.002$ ) and hip (42%;  $P=0.003$ ) at the second ipsilateral step (Figure 3C). Subjects also  
117 absorbed significantly greater peak power at the ankle (44%;  $P=0.001$ ), knee (50%;  $P=0.003$ )  
118 and hip (64%;  $P=0.014$ ) at the second ipsilateral step (Figure 3D). There was no significant main  
119 effect for starting positions or significant interaction.

#### 120 **4. Discussion**

121 Due to enhanced momentum when initiating stair ascent from a walk (increased velocity)  
122 compared to initiating stair ascent from a stand, we hypothesized that the frontal plane joint  
123 dynamics would be greater as one ascends stairs from a walk and such differences would be  
124 augmented in the next ipsilateral step. Collectively, our results supported both hypotheses. The  
125 greater peak knee abductor moment when initiating stair ascent from a walk demonstrates that  
126 the lateral portions of the knee experience higher levels of stress. Greater peak hip abductor  
127 moment when initiating stair ascent from a walk (Figure 3A) indicates an increased activity of  
128 the ipsilateral hip abductors. This increased activity could assist the contralateral limb to avoid  
129 contact with the intermediate step by counteracting the pelvic drop on the contralateral side  
130 (Kirkwood et al., 1999; Nadeau et al., 2003). Also, initiating stair ascent from a walk could have  
131 resulted in greater velocity and hence greater peak joint moments at knee and hip joints. Based  
132 on previous literature, a 3% difference between the peak knee abductor moments during both the  
133 conditions might only be statistical (Costigan et al., 2002). However, the 7% difference between  
134 the peak hip abductor moments suggests that ascending stairs from a walk could be more  
135 challenging compared to ascending stairs from a stand (Nadeau et al., 2003). This could be an  
136 important finding in the literature concerning people with weaker hip abductors, e.g. hip  
137 arthroplasty and osteoarthritis. Such individuals may not be able to generate sufficient moments

138 to counteract the pelvic drop on the contralateral side, possibly resulting in a mechanically  
139 inefficient stair ascent. Similar joint powers in both conditions could indicate greater angular  
140 velocity at the knee and hip joints during the second condition. Also, similar peak ankle joint  
141 moments and powers between the two conditions could be due to the relatively small  
142 contribution of the ankle joint to frontal plane stability while ascending stairs (Nadeau et al.,  
143 2003).

144 Greater peak moments and powers while ascending the second ipsilateral step (Figures  
145 3B-D) highlight the greater effort needed to maintain stability in the frontal plane or to help the  
146 contralateral leg move to clear the intermediate step as one ascends. Electromyography data in  
147 future studies could highlight how different muscle loadings contribute to this greater effort. The  
148 joint moment profiles and values in the current study were similar to the ones reported in the  
149 literature (Kirkwood et al., 1999; Nadeau et al., 2003; Novak and Brouwer, 2011; Table 1). The  
150 three lower-extremity joints largely experienced abductor moments throughout the stance phase  
151 (Figure 4). One plausible reason is the passage of the ground reaction force vector medially with  
152 respect to the joint centers (Kirkwood et al., 1999).

## 153 **5. Conclusion**

154 Results from the present study demonstrated that the knee and hip joints experience greater  
155 peak abductor moments when initiating stair ascent from a walk and at the next ipsilateral step.  
156 These findings could provide therapists a comprehensive understanding of the mechanisms  
157 involved during stair climbing when used as a training/testing module for evaluating hip  
158 strength. In addition, results have methodological implications for the stair negotiation  
159 biomechanical research, especially in individuals with documented frontal plane abnormalities  
160 (i.e. knee and hip osteoarthritis, ACL injury).



161 **References**

- 162 Andriacchi, T.P., Andersson, G.B., Fermier, R.W., Stern, D., Galante, J.O., 1980. A study of  
163 lower-limb mechanics during stair-climbing. *J Bone Joint Surg Am.* 62 (5), 749-757.
- 164 Costigan, P.A., Deluzio, K.J., Wyss, U.P., 2002. Knee and hip kinetics during normal stair  
165 climbing. *Gait Posture.* 16 (1), 31-37.
- 166 Hemenway, D., Solnick, S.J., Koeck, C., Kytir, J., 1994. The incidence of stairway injuries in  
167 Austria. *Accid Anal Prev.* 26 (5), 675-679.
- 168 Holsgaard-Larsen, A., Caserotti, P., Puggaard, L., Aagaard, P., 2011. Stair-ascent performance in  
169 elderly women: effect of explosive strength training. *J Aging Phys Act.* 19 (2): 117-136.
- 170 Houck, J.R., Duncan, A., De Haven, K.E., 2005. Knee and hip angle and moment adaptations  
171 during cutting tasks in subjects with anterior cruciate ligament deficiency classified as  
172 noncopers. *J Orthop Sports Phys Ther.* 35 (8), 531-540.
- 173 Kirkwood, R.N., Culham, E.G., Costigan, P., 1999. Hip moments during level walking, stair  
174 climbing, and exercise in individuals aged 55 years or older. *Phys Ther.* 79 (4), 360-370.
- 175 Kowalk, D. L., Duncan, J.A., Vaughan, C. L., 1996. Abduction-adduction moments at the knee  
176 during stair ascent and descent. *J Biomech.* 29 (3), 383-388.
- 177 McFadyen, B.J., Winter, D.A., 1988. An integrated biomechanical analysis of normal stair ascent  
178 and descent. *J Biomech.* 21 (9), 733-744.
- 179 Nadeau, S., McFadyen, B.J., Malouin, F., 2003. Frontal and sagittal plane analysis of the stair  
180 climbing task in healthy adults aged over 40 years: what are the challenges compared to  
181 level walking? *Clin Biomech.* 18 (10), 950-959.
- 182 Novak, A. C., Brouwer, B., 2011. Sagittal and frontal lower limb joint moments during stair  
183 ascent and descent in young and older adults. *Gait Posture.* 33 (1), 54-60.

184 Reeves, N.D., Spanjaard, M., Mohagheghi, A.A., Baltzopoulos, V., Maganaris, C.N., 2008.  
185 Influence of light handrail use on the biomechanics of stair negotiation in old age. *Gait*  
186 *Posture*. 28 (2), 327-336.

187 Rubenstein, L.Z., 2006. Falls in older people: epidemiology, risk factors and strategies for  
188 prevention. *Age Ageing*. 35(suppl 2): ii37-ii41.

189 Startzell, J.K., Owens, D.A., Mulfinger, L.M., Cavanagh, P.R., 2000. Stair negotiation in older  
190 people: A review. *J Am Geriatr Soc*. 48 (5), 567-580.

191 Vallabhajosula, S., Yentes, J.M., Momcilovic, M., Blanke, D.J., Stergiou, N., 2011. Do lower-  
192 extremity joint dynamics change when stair negotiation is initiated with a self-selected  
193 comfortable gait speed? *Gait Posture* (in press)  
194  
195