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1 **Frontal Joint Dynamics when Initiating Stair Ascent from a Walk versus a Stand**
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22

23 **Abstract**

24 Ascending stairs is a challenging activity of daily living for many populations. Frontal plane
25 joint dynamics are critical to understand the mechanisms involved in stair ascension as they
26 contribute to both propulsion and medio-lateral stability. However, previous research is limited
27 to understanding these dynamics while initiating stair ascent from a stand. We investigated if
28 initiating stair ascent from a walk with a comfortable self-selected speed can affect the frontal
29 plane lower-extremity joint moments and powers as compared to initiating stair ascent from a
30 stand and if this difference would exist at consecutive ipsilateral steps on the stairs. Kinematics
31 data using a 3-D motion capture system and kinetics data using two force platforms on the first
32 and third stair treads were recorded simultaneously as ten healthy young adults ascended a
33 custom-built staircase. Data were collected from two starting conditions of stair ascent, from a
34 walk (speed: $1.42 \pm 0.21 \text{ m/s}$) and from a stand. Results showed that subjects generated greater
35 peak knee abductor moment and greater peak hip abductor moment when initiating stair ascent
36 from a walk. Greater peak joint moments and powers at all joints were also seen while ascending
37 the second ipsilateral step. Particularly, greater hip abductor moment was needed to avoid
38 contact of the contralateral limb with the intermediate step by counteracting the pelvic drop on
39 the contralateral side. This could be important for therapists using stair climbing as a
40 testing/training tool to evaluate hip strength in individuals with documented frontal plane
41 abnormalities (i.e. knee and hip osteoarthritis, ACL injury).

42 **Keywords:** Stair climbing; Joint moments; Joint powers; Walking; Stair ambulation;
43 Abductor Muscles; Adductor Muscles

44

45

46 **1. Introduction**

47 Older adults frequently experience falls while negotiating stairs (Rubenstein 2006;
48 Hemenway et al., 1994). Hence, understanding fall-related mechanisms via examining the joint
49 dynamics (moments and powers) has been a research area of great interest (McFadyen and
50 Winter, 1988; Startzell et al., 2000; Reeves et al., 2008). Particularly, the frontal plane dynamics
51 contribute to both propulsion and medio-lateral stability (Nadeau et al., 2003; Novak and
52 Brouwer, 2011) and are critical at the knee and hip joints (Andriacchi et al., 1980; Kowalk et al.,
53 1996; Costigan et al., 2002). These two joints experience external adductor moments (Kowalk et
54 al., 1996) and compared to level-walking, these moments are lesser at the hip and greater at the
55 knee (Costigan et al., 2002; Nadeau et al., 2003). These moments have also been shown to be
56 similar for two consecutive steps (Kowalk et al., 1996). Examining the frontal plane dynamics
57 during stair negotiation could play a pivotal role in rehabilitation of people with weak hip
58 abductors and with knee problems (Nadeau et al., 2003).

59 Importantly, the currently available literature only includes studies where stair ascent was
60 initiated from a stand. However, initiating stair ascent from a walk is much more common at
61 private and public locations. Thus to increase external validity in the stair negotiation research, it
62 is important to consider such a condition. Such an approach immediately generates several
63 crucial questions: Does ascending stairs from a walk require greater moments and more power to
64 maintain frontal plane stability as compared to initiating stair ascent directly from a stand? And
65 if such differences exist, are they present only at the first step of the staircase or also at the next
66 ipsilateral step? Previous work has shown that ascending stairs starting from a walk caused
67 higher peak knee and hip extensor moments in the sagittal plane as compared to starting stair
68 ascent from a stand and altered lower-extremity joint moments and powers between two

69 consecutive ipsilateral steps (Vallabhajosula et al., in press). Such differences could also result in
70 different joint moments and powers to maintain medio-lateral stability during stair ascent after
71 starting from a walk or a stand. Therefore, the objective of the present study was to determine
72 frontal plane joint dynamics when one ascends stairs from a walk compared to ascending stairs
73 from a stand. Due to enhanced momentum when initiating stair ascent from a walk (increased
74 velocity) compared to initiating stair ascent from a stand, we hypothesized that the frontal plane
75 joint moments and powers will be greater when 1) ascending stairs from a walk and 2) at the next
76 ipsilateral step.

77 **2. Methods**

78 Ten healthy subjects (three females; 26.4 ± 3.7 years; 76.2 ± 13.6 kg; 1.78 ± 0.08 m) signed an
79 informed consent approved by the local institutional review board. Inclusion criteria were: age
80 between 19-35 years and free of any injury that could alter gait. Exclusion criteria were: presence
81 of any known disorder(s) that may affect gait or the inability to negotiate a stairway.

82 Kinematic (Motion Analysis Corp., Santa Rosa, CA; 60 Hz) and kinetic data using two
83 force platforms embedded in the first and the third stair treads of an instrumented stairway
84 (Advanced Mechanical Technology Inc., Watertown, MA; 600 Hz) were collected (Figure 1).
85 The force platforms were isolated from the rest of the structure to avoid vibration artifacts
86 (similar to Holsgaard-Larsen et al., 2011).

87 Retro-reflective markers were placed on subjects' pelvis and lower limbs based on
88 modified Helen Hayes marker set (Houck et al., 2005). Before testing, all the subjects were
89 allowed to practice stair ascension without using handrails. During testing, none of the subjects
90 used the handrails. Subjects wore comfortable sport shoes and walked towards the stairs at their
91 self-selected comfortable speed from a distance of 5m. Their speed was calculated based on the

92 time recordings of two photocells positioned 2m apart in front of the stairway (Figures 2A,2B).
93 An average walking speed (1.42 ± 0.21 m/s) from 16 such trials was used as the self-selected
94 comfortable speed for each subject. Next, the subjects ascended stairs five times in two
95 conditions, starting with the right limb for each condition: 1) initiating stair ascent from a walk
96 (condition 1; Figures 2A,2B), and 2) initiating stair ascent from a stand (condition 2; Figures
97 2C,2D). An acceptable trial for condition 1 required the subject to ascend the stairway within
98 $\pm 10\%$ of the self-selected comfortable speed. Data were collected until five acceptable trials
99 were procured. The order of the conditions was randomized.

100 Peak internal abductor and adductor moments, and peak power generated and absorbed at
101 ankle, knee, and hip joints were used as the dependent variables (Costigan et al., 2002; Nadeau et
102 al., 2003). They were calculated for two consecutive ipsilateral steps on the staircase during both
103 conditions using a custom-written Matlab (MathWorks Inc., Natick, MA, USA) program. For
104 each subject, and for each condition, the maximum and minimum joint moments and powers
105 from the five trials were averaged to calculate the mean values. Group means and standard
106 deviations were then obtained by averaging these mean peak values. A fully repeated two-way
107 ANOVA (condition X step) was performed using SPSS (International Business Machines,
108 Armonk, NY) with α -value set at 0.05.

109 3. Results

110 Subjects produced significantly greater peak abductor moments at the knee (3%; $P=0.014$)
111 and hip (7%; $P=0.006$) when initiating stair ascent from a walk (Figure 3A). Subjects produced
112 significantly greater peak ankle (20%; $P=0.007$), knee (20%; $P<0.001$) and hip abductor
113 moments (20%; $P<0.001$) at the second ipsilateral step (Figure 3B). There were no significant
114 interactions.

115 Subjects generated significantly greater peak power at the ankle (48%; $P=0.023$), knee (43%;
116 $P=0.002$) and hip (42%; $P=0.003$) at the second ipsilateral step (Figure 3C). Subjects also
117 absorbed significantly greater peak power at the ankle (44%; $P=0.001$), knee (50%; $P=0.003$)
118 and hip (64%; $P=0.014$) at the second ipsilateral step (Figure 3D). There was no significant main
119 effect for starting positions or significant interaction.

120 **4. Discussion**

121 Due to enhanced momentum when initiating stair ascent from a walk (increased velocity)
122 compared to initiating stair ascent from a stand, we hypothesized that the frontal plane joint
123 dynamics would be greater as one ascends stairs from a walk and such differences would be
124 augmented in the next ipsilateral step. Collectively, our results supported both hypotheses. The
125 greater peak knee abductor moment when initiating stair ascent from a walk demonstrates that
126 the lateral portions of the knee experience higher levels of stress. Greater peak hip abductor
127 moment when initiating stair ascent from a walk (Figure 3A) indicates an increased activity of
128 the ipsilateral hip abductors. This increased activity could assist the contralateral limb to avoid
129 contact with the intermediate step by counteracting the pelvic drop on the contralateral side
130 (Kirkwood et al., 1999; Nadeau et al., 2003). Also, initiating stair ascent from a walk could have
131 resulted in greater velocity and hence greater peak joint moments at knee and hip joints. Based
132 on previous literature, a 3% difference between the peak knee abductor moments during both the
133 conditions might only be statistical (Costigan et al., 2002). However, the 7% difference between
134 the peak hip abductor moments suggests that ascending stairs from a walk could be more
135 challenging compared to ascending stairs from a stand (Nadeau et al., 2003). This could be an
136 important finding in the literature concerning people with weaker hip abductors, e.g. hip
137 arthroplasty and osteoarthritis. Such individuals may not be able to generate sufficient moments

138 to counteract the pelvic drop on the contralateral side, possibly resulting in a mechanically
139 inefficient stair ascent. Similar joint powers in both conditions could indicate greater angular
140 velocity at the knee and hip joints during the second condition. Also, similar peak ankle joint
141 moments and powers between the two conditions could be due to the relatively small
142 contribution of the ankle joint to frontal plane stability while ascending stairs (Nadeau et al.,
143 2003).

144 Greater peak moments and powers while ascending the second ipsilateral step (Figures
145 3B-D) highlight the greater effort needed to maintain stability in the frontal plane or to help the
146 contralateral leg move to clear the intermediate step as one ascends. Electromyography data in
147 future studies could highlight how different muscle loadings contribute to this greater effort. The
148 joint moment profiles and values in the current study were similar to the ones reported in the
149 literature (Kirkwood et al., 1999; Nadeau et al., 2003; Novak and Brouwer, 2011; Table 1). The
150 three lower-extremity joints largely experienced abductor moments throughout the stance phase
151 (Figure 4). One plausible reason is the passage of the ground reaction force vector medially with
152 respect to the joint centers (Kirkwood et al., 1999).

153 **5. Conclusion**

154 Results from the present study demonstrated that the knee and hip joints experience greater
155 peak abductor moments when initiating stair ascent from a walk and at the next ipsilateral step.
156 These findings could provide therapists a comprehensive understanding of the mechanisms
157 involved during stair climbing when used as a training/testing module for evaluating hip
158 strength. In addition, results have methodological implications for the stair negotiation
159 biomechanical research, especially in individuals with documented frontal plane abnormalities
160 (i.e. knee and hip osteoarthritis, ACL injury).

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